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# Repeatability and Reproducibility of Foveal Avascular Zone Area Measurement on Normal Eyes by Different Optical Coherence Tomography Angiography Instruments

Elisabetta Pilotto<sup>a</sup> Luisa Frizziero<sup>b</sup> Anna Crepaldi<sup>a</sup> Enrico Della Dora<sup>a</sup> Davide Deganello<sup>a</sup> Evelyn Longhin<sup>a</sup> Enrica Convento<sup>a</sup> Raffaele Parrozzani<sup>a</sup> Edoardo Midena<sup>a, b</sup>

<sup>a</sup>Department of Ophthalmology, University of Padova, Padova, Italy; <sup>b</sup>G.B. Bietti Foundation, IRCCS, Rome, Italy

## Keywords

Optical coherence tomography angiography · Foveal avascular zone area · Superficial retinal capillary plexus · Deep retinal capillary plexus

# Abstract

Purpose: To compare the foveal avascular zone (FAZ) area measurements produced by different optical coherence tomography angiography (OCTA). *Methods:* Healthy enrolled volunteers underwent OCTA using 2 different devices: Spectralis HRA+OCTA (Heidelberg Engineering, Heidelberg, Germany) and RS-3000 Advance (Nidek, Gamagori, Japan). Two graders measured FAZ in both superficial (SCP) and deep (DCP) retinal capillary plexuses. The SCP and DCP en face images were visualized automatically segmenting 2 separate slabs defined by the arbitrary segmentation lines created by the software of each OCT device. One grader repeated each measure twice. Results: Fifty-nine eyes were included. The mean FAZ was 0.33  $\pm$  0.09 mm<sup>2</sup> at the SCP and 0.57  $\pm$  0.17  $mm^2$  at the DCP measured with RS-3000 versus 0.30  $\pm$  0.08 and  $0.35 \pm 0.08$  mm<sup>2</sup>, respectively, measured with Spectralis. The measurements of the 2 devices were significantly different (p < 0.0001). The intraoperator agreement was excellent

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E-Mail karger@karger.com www.karger.com/ore at the SCP (intraclass correlation coefficient, ICC: 0.97 with Spectralis and 0.96 with RS-3000). At the DCP, it was good with Spectralis and fair with RS-3000 (ICC: 0.85 and 0.64, respectively). The interoperator agreement was excellent for Spectralis and good for RS-3000 at the SCP (ICC: 0.97 and 0.93, respectively). It was good at the DCP with both devices (ICC: 0.74 with RS-3000 and 0.81 with Spectralis). **Conclusions:** FAZ measurements obtained with different OCTA devices differ. These findings should be considered in followup studies of patients with retinal vascular diseases.

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#### Introduction

Optical coherence tomography angiography (OCTA) is a newly developed noninvasive imaging technique, allowing en face visualization in vivo and separately of both superficial (SCP) and deep retinal capillary plexuses (DCP) [1, 2]. Moreover, OCTA allows us to detect and measure the foveal avascular zone (FAZ) area, which may

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Edoardo Midena, MD Department of Ophthalmology, University of Padova Via Giustiniani 2 IT-35128 Padova (Italy) E-Mail edoardo.midena@unipd.it be affected in several retinal vascular diseases. Therefore, FAZ area measurement must be a reliable and repeatable method. The aim of this study was to compare FAZ area measurements produced by two different optical OCTA devices when imaging normal eyes.

### Methods

#### Study Design and Population

This prospective cross-sectional study, compliant with the tenets of the Declaration of Helsinki, was approved by our institutional review board (IRB), and written informed consent was obtained. Subjects were recruited between September and November 2016 at our institute. Inclusion criteria were healthy volunteers aged 18 years or older with normal visual acuity (best-corrected visual acuity of 20/20 or better) and spherical equivalent less than 3 dpt. Exclusion criteria were any history or clinical evidence of ocular and/or systemic diseases, any previous ocular surgery or laser treatment, and media opacities precluding adequate fundus imaging.

#### Data Acquisition

All subjects underwent full ophthalmological examination. Both eyes of all subjects underwent OCTA using 2 different devices: Spectralis HRA+OCTA (Heidelberg Engineering, Heidelberg, Germany) and RS-3000 Advance (Nidek, Gamagori, Japan). For each subject, both examinations were performed during the same day in the early afternoon.

Spectralis has an A-scan rate of 70,000 scans/s, using a light source centered on 870 nm, with an axial and transverse resolution of 3.9 and 6  $\mu$ m in tissue. An OCTA scan pattern of 15 × 5 degrees (44 × 1.5 mm; consisting of 131 B-scans separated by 11  $\mu$ m) centered on the fovea was acquired. The OCTA image automated realtime mode was settled at 35 (frames averaged per B-scan). The SCP and the DCP en face images were visualized automatically segmenting 2 separate slabs defined by the arbitrary segmentation lines created by the software of the device: a superficial slab extending from the inner limiting membrane (ILM) to the outer border of the inner plexiform layer (IPL) for the SCP, and a deeper one from the outer border of the IPL to the outer border of the outer plexiform layer (OPL) for the DCP.

The RS-3000 Advance has an A-scan rate of 53,000 scans/s, using a light source centered on 880 nm, with an axial and transverse resolution of 7 and 20  $\mu$ m in tissue. The Angioscan 8 OCTA software was used for acquisition of a 3 × 3 mm macular map, consisting of 256 B-scans separated by 11  $\mu$ m. The bright intensity score of the image, which may range from –10 to +10, was settled at 0, as usually automatically provided by the device itself. The SCP and the DCP en face images were visualized automatically segmenting 2 separate slabs defined by the arbitrary segmentation lines created by the software of the device: a slab extending from the ILM to 8  $\mu$ m below the inner boundary of the inner nuclear layer (INL) for the SCP, and a deeper one from 12  $\mu$ m below the inner boundary of the INL to a segmenting line localized 86  $\mu$ m below for the DCP.

All images from the 2 devices were reviewed to confirm consistent segmentation by the automated instrument software. In all images automated segmentation was correct and no manual resegmentation was necessary. Poor-quality images (quality index lower than 35 dB for Spectralis and signal strength index lower than 7 for RS-3000 Advance) were excluded. The enface images of the SCP and DCP were automatically generated by the inbuilt software of both devices (Fig. 1).

#### Data Analysis and Study Setting

Two well-trained graders (A.C. and E.D.D) independently measured the FAZ area, defined as the avascular area in the center of the fovea, in a random sequence. The inbuilt automatic area measurement editor of both devices was used (Fig. 1) One of the two graders repeated each measure twice at 1 week apart.

#### Statistical Analysis

Intra- and interoperator agreement were graded considering the absolute value of the intraclass correlation coefficient (ICC) and the confidence interval. For the assessment of reproducibility, data of grader A.C. and first measurement data of grader E.D.D. were used. A Bland-Altman plot was constructed by plotting each test-retest difference against its mean.

Mann-Whitney and Friedman nonparametric tests were used for comparison between 2 groups and among more than 2 groups, respectively. Linear regression analysis evaluated the linear association between the test-retest score difference and the X value. Statistical analyses were performed using SAS version 9.3 software (SAS Institute, Cary, NC, USA).

## Results

A total of 33 subjects were enrolled (17 males, 16 females; mean age:  $26 \pm 3$  years). OCTA en face images of 59 eyes were included. Seven eyes (10.6%) were excluded because of poor OCT image quality. The mean FAZ area was  $0.33 \pm 0.09 \text{ mm}^2$  at the SCP and  $0.57 \pm 0.17 \text{ mm}^2$  at the DCP measured with RS-3000 versus  $0.30 \pm 0.08$  and  $0.35 \pm 0.08 \text{ mm}^2$ , respectively, measured with Spectralis. The measurements of the 2 devices were significantly different both at the SCP and at the DCP (both p < 0.0001).

The intraoperator agreement was excellent with both devices at the SCP: ICC = 0.96 (95% CI: 0.93-0.98) with RS-3000 and 0.97 (95% CI: 0.93-0.98) with Spectralis. At the DCP, the intraoperator agreement was good with Spectralis: ICC = 0.85 (95% CI: 0.62-0.93), and fair with RS-3000: ICC = 0.64 (95% CI: 0.33-0.81). The intraoperator agreement was corroborated by Bland-Altman analysis (Fig. 2).

The interoperator agreement was excellent for Spectralis: ICC = 0.97 (95% CI: 0.93-0.98), and good for RS-3000: ICC = 0.93 (95% CI: 0.57-0.98) at the SCP. It was good at the DCP with both devices: ICC = 0.74 (95% CI: 0.52-0.87) with RS-3000 and 0.81 (95% CI: 0.63-0.91) with Spectralis. The interoperator agreement was corroborated by Bland-Altman analysis (Fig. 3).



**Fig. 1.** En face images of the superficial (SCP) (**a**–**d**) and deep capillary plexus (DCP) (**e**–**h**) from Spectralis (**a**, **b**, **e**, **f**) and RS-3000 (**c**, **d**, **g**, **h**). The SCP image was visualized automatically segmenting a superficial slab extending from the inner limiting membrane (ILM) to the outer border of the inner plexiform layer (IPL) for the Spectralis (**i**) and from the ILM to 8 µm below the inner boundary of the inner nuclear layer (INL) for the RS-3000 (**k**). The DCP im-

#### age was visualized automatically segmenting a deeper slab extending from the IPL outer border to the outer plexiform layer (OPL) outer border for the Spectralis (**j**) and from 12 $\mu$ m below the inner boundary of the INL to a segmenting line localized 86 $\mu$ m below for the RS-3000 (**I**). The FAZ area was automatically measured and visualized with different colors for the 2 graders (blue and yellow for Spectralis and green and rose for RS-3000).

# Discussion

The advent of OCTA has appraised the interest in configuration and quantification of the FAZ area [1-8]. The FAZ enlargement rate, identified using fluorescein angiography, is an indicator of the progression of macular ischemia [9, 10]. When comparing fluorescein angiography and OCTA in the classification of diabetic retinopathy, OCTA allows better discrimination of FAZ disruption and capillary dropout in the superficial retinal layers [11]. Moreover, OCTA can separately visualize the SCP and the DCP; therefore, the possible different involvement of FAZ in these 2 plexuses is under investigation [6]. In agreement with the findings of Carpineto et al. [12] and Mastropasqua et al. [13], we detected excellent repeatability and reproducibility in FAZ area measurement when measuring the FAZ at the SCP [12, 13]. On the contrary, repeatability and reproducibility were lower when measuring the FAZ area at the DCP, in agreement with the finding of Ghasemi Falavarjani et al. [6]. FAZ limits can be clearly identified at the more superficial layer,

whereas in the deeper retina the edge points along the centerline of the vessels are more difficult to delineate. Campbell et al. [16], using a novel OCTA algorithm, visualized that around the FAZ the retinal plexuses converge to form a single parafoveal capillary loop and collectively define the FAZ borders, in agreement with early histological studies in primates [14, 15]. Therefore, the authors recommend that the FAZ size be measured using an en face projection that includes all retinal plexuses [16].

In the present study we included only healthy eyes. Therefore, automated segmentation was correct in all images and no manual resegmentation was necessary. We may expect that in nonhealthy eyes, when intraretinal pathological changes are present, automatic segmentation may result in compromising measurement repeatability.

In the present study we compared FAZ measurements obtained by 2 different OCTA instruments, detecting that the measurements of the 2 devices were significantly different at both plexuses. We used the OCTA en face



**Fig. 2.** Bland-Altman plot analysis of intraoperator repeatability. A nonsignificant bias resulted for the superficial capillary plexus (SCP) both for RS-3000 (**a**) and Spectralis (**c**) (mean: 0.007 and -0.001, respectively). A bigger but always limited bias was shown for the deep capillary plexus (DCP) for RS-3000 (**b**) and Spectralis (**d**) (mean: 0.072 and 0.029, respectively). No significant trend was evident. The narrowest agreement ranges were always shown for

Spectralis compared to RS-3000 for both SCP and DCP (0.067 for Spectralis and 0.215 for RS-3000 at the SCP; 0.251 for Spectralis and 0.46 for RS-3000 at the DCP). In every plot 95% of the measured differences were within the range; in particular, they were all within the range when evaluating SCP with Spectralis. OD, oculus dextrus (right eye); OS, oculus sinister (left eye).

images of the SCP and DCP, automatically generated by the devices, for the measurement. However, the instruments use different extending slabs to identify them. To image the SCP, the RS-3000 sets the outer border of the slab deeper than that adopted by the Spectralis (Fig. 1). Campbell et al. [16] were able to confirm in vivo the presence of 3 vascular plexuses previously described in primate histological studies: 1 SCP and 2 additional capillary plexuses, 1 on either side of the INL (the intermediate capillary plexus [ICP] and the DCP) [14, 16]. A deeper superficial slab, including more packed vessels than both the SCP and the ICP, could explain the major

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**Fig. 3.** Bland-Altman plot analysis of interoperator agreement. A nonsignificant bias resulted both for RS-3000 (**a**, **b**) and Spectralis (**c**, **d**), analyzing both the superficial capillary plexus (SCP) (mean: 0.023 and -0.005, respectively) and the deep capillary plexus (DCP) (mean: 0.005 and -0.023, respectively). No significant trend was evident. The narrowest agreement ranges were shown for the SCP (0.076 for Spectralis and 0.088 for RS-3000). For the DCP, the

agreement range was slightly narrower for Spectralis compared to RS-3000 (0.287 for Spectralis and 0.357 for RS-3000). In every analysis, 95% of differences were within the range at SCP, while they were at the limit when analyzing the foveal avascular zone at the DCP with RS-3000 (5%) and slightly outside with Spectralis (8%). OD, oculus dextrus (right eye); OS, oculus sinister (left eye).

discrepancy between the RS-3000 and the Spectralis measurements we detected at the SCP and DCP. The main limitation of the present study is the small sample size.

In conclusion, FAZ measurements obtained with different OCTA devices are different. These differences appear to be primarily attributable to the different analysis algorithms used to set the SCP and DCP. These findings should be taken into consideration when separately studying the FAZ area in different retinal layers or when planning a follow-up study.

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#### References

- Spaide RF, Curcio CA: Evaluation of segmentation of the superficial and deep vascular layers of the retina by optical coherence tomography angiography instruments in normal eyes. JAMA Ophthalmol 2017;135:259–262.
- 2 Savastano MC, Lumbroso B, Rispoli M: In vivo characterization of retinal vascularization morphology using optical coherence tomography angiography. Retina 2015;35: 2196–2203.
- 3 Pakzad-Vaezi K, Keane PA, Cardoso JN, Egan C, Tufail A: Optical coherence tomography angiography of foveal hypoplasia. Br J Ophthalmol 2017;101:985–988.
- 4 Bonnin S, Mané V, Couturier A, Julien M, Paques M, Tadayoni R, Gaudric A: New insight into the macular deep vacular plexus imaged by optical coherence tomography angiography. Retina 2015;35:2347–2352.
- 5 Ishibazawa A, Nagaoka T, Takahashi A, Omae T, Tani T, Sogawa K, Yokota H, Yoshida A: Optical coherence tomography angiography in diabetic retinopathy: a prospective pilot study. Am J Ophthalmol 2015;160:35– 44.e1.
- 6 Ghasemi Falavarjani K, Iafe NA, Hubschman JP, Tsui I, Sadda SR, Sarraf D: Optical coherence tomography angiography analysis of the foveal avascular zone and macular vessel den-

sity after anti-VEGF therapy in eyes with diabetic macular edema and retinal vein occlusion. Invest Ophthalmol Vis Sci 2017;58:30–34.

**Disclosure Statement** 

mitted paper.

- 7 Feucht N, Schönbach EM, Lanzl I, Kotliar K, Lohmann CP, Maier M: Changes in the foveal microstructure after intravitreal bevacizumab application in patients with retinal vascular disease. Clin Ophthalmol 2013;7: 173–178.
- 8 Michaelides M, Fraser-Bell S, Hamilton R, et al: Macular perfusion determined by fundus fluorescein angiography at the 4-month time point in a prospective randomized trial of intravitreal bevacizumab or laser therapy in the management of diabetic macular edema (Bolt Study): report 1. Retina 2010;30: 781–786.
- 9 Arend O, Wolf S, Harris A, Reim M: The relationship of macular microcirculation to visual acuity in diabetic patients. Arch Ophthalmol 1995;113:610–614.
- 10 Sim DA, Keane PA, Zarranz-Ventura J, et al: Predictive factors for the progression of diabetic macular ischemia. Am J Ophthalmol 2013;156:684–692.
- 11 Soares M, Neves C, Marques IP, Pires I, Schwartz C, Costa MÂ, Santos T, Durbin M, Cunha-Vaz J: Comparison of diabetic reti-

nopathy classification using fluorescein angiography and optical coherence tomography angiography. Br J Ophthalmol 2017;101:62– 68.

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- 12 Carpineto P, Mastropasqua R, Marchini G, Toto L, Di Nicola M, Di Antonio L: Reproducibility and repeatability of foveal avascular zone measurements in healthy subjects by optical coherence tomography angiography. Br J Ophthalmol 2016;100:671–676.
- 13 Mastropasqua R, Toti L, Mattei PA, et al: Reproducibility and repeatability of foveal avascular zone area measurements using sweptsource optical coherence tomography angiography in healthy subjects. E J Ophthalmol 2017;27:336–341.
- 14 Snodderly DM, Weinhaus RS, Choi JC: Neural-vascular relationships in central retina of macaque monkeys (*Macaca fascicularis*). J. Neurosci 1992;12:1169–1193.
- 15 Weinhaus RS, Burke JM, Delori FC, Snodderly DM: Comparison of fluorescein angiography with microvascular anatomy of macaque retinas. Exp. Eye Res 1995;61:1–16.
- 16 Campbell JP, Zhang M, Hwang TS, Bailey ST, Wilson DJ, Jia Y, Huang D: Detailed vascular anatomy of the human retina by projectionresolved optical coherence tomography angiography. Sci Rep 2017;7:42201.

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