



# Behavioural stochastic resonance across the lifespan

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## Abstract

Stochastic resonance (SR) is the phenomenon wherein the introduction of a suitable level of noise enhances the detection of subthreshold signals in non linear systems. It manifests across various physical and biological systems, including the human brain. Psychophysical experiments have confirmed the behavioural impact of stochastic resonance on auditory, somatic, and visual perception. Aging renders the brain more susceptible to noise, possibly causing differences in the SR phenomenon between young and elderly individuals. This study investigates the impact of noise on motion detection accuracy throughout the lifespan, with 214 participants ranging in age from 18 to 82. Our objective was to determine the optimal noise level to induce an SR-like response in both young and old populations. Consistent with existing literature, our findings reveal a diminishing advantage with age, indicating that the efficacy of noise addition progressively diminishes. Additionally, as individuals age, peak performance is achieved with lower levels of noise. This study provides the first insight into how SR changes across the lifespan of healthy adults and establishes a foundation for understanding the pathological alterations in perceptual processes associated with aging.

**Keywords** Stochastic resonance · Neural noise · Visual perception · Ageing · Psychophysics

## Introduction

Surprisingly, introducing a specific amount of noise to a subthreshold stimulus can improve signal detectability—a phenomenon known as stochastic resonance (SR) (McDonnell & Abbott, 2009; Moss & Wiesenfeld, 1995; Moss et al., 2004). One practical application of SR is observed in image restoration, where controlled, typically low-level noise is strategically introduced to a degraded image. This carefully calibrated noise interacts with existing image information,

serving as a catalyst to amplify weak or subtle features (Kojima et al., 2019).

In investigating SR-like phenomena through behavioural tasks, plotting individual performance against external noise levels reveals a characteristic inverted U-shaped function (McDonnell & Abbott, 2009), indicating optimal performance at an intermediate level of noise (Moss et al., 2004; Simonotto et al., 1997). Concerning the mechanism at the basis of SR, the energy of the noise acts like a pedestal (Moss et al., 2004). Consequently, in the absence of noise, the energy of the stimulus is insufficient for detection. By adding the optimal amount of noise, the total energy (signal + noise) rises above the threshold and the stimulus becomes detectable. Conversely, when the noise is too high, it overwhelms the signal, causing a degradation in performance. When the amount of noise is on the sweet spot, the peak performance is achieved (van der Groen et al., 2018).

The term SR, initially introduced in the realm of physics, has garnered attention across various perceptual domains. For instance, in the sensorimotor domain, Mendez-Balbuena et al. (2012) illustrated that applying mechanical noise at varying levels to participants' arms enhanced motor output at moderate noise levels. Similarly, Zeng et al. (2000) demonstrated auditory SR by using white noise to aid speech

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perception in hearing-impaired individuals, finding that specific noise intensities improved recognition capabilities, thereby supporting the application of SR in auditory assistive technologies. In tactile domains, Collins et al. (1996) manipulated mechanical noise intensities applied to the fingertip, which enhanced the detection of weak tactile stimuli. Vestibular SR was examined by Iwasaki et al. (2014) and Mulavara et al. (2011), who found that noise could enhance postural stability, suggesting potential applications in balance disorder rehabilitation.

Visual SR has been extensively investigated through various methods, including computational modelling, laboratory experiments, and brain stimulation techniques (Kim et al., 2006; van Boxtel, 2019; Ward et al., 2002, 2006; Yamazaki & Lioumis, 2022). Simonotto et al. (1997) showed that an appropriate amount of noise (gaussian noise) led to improvements in contrast detection of a digitized picture of Big Ben. Runnova et al. (2016) introduced the concept of “effective noise intensity” to quantify brain activity during the perception of ambiguous images, such as the Necker cube, confirming that optimal noise levels could indeed enhance visual perception. Studies by Kundu and Sarkar (2015) and Sasaki et al. (2006) focused on contrast sensitivity enhancements due to SR, whereas Treviño et al. (2016) and Itzcovich et al. (2017) expanded this research to motion perception and clinical populations, respectively. Itzcovich et al. (2017) found that noise could assist in motion perception tasks for individuals with visual impairments.

In the field of neuroscience, an ongoing debate surrounds the question of whether the brain has evolved to incorporate random noise in vivo as part of the “neural code.” This idea is supported by indirect evidence of a positive role for noise in the brain (McDonnell & Abbott, 2009). However, this hypothesis is complicated by the existence of various sources of noise that interact together. For instance, *external noise* includes irrelevant perceptual stimuli, whereas *neural noise* encompasses random fluctuations in brain activity at both the single cell level and the neural network level (Dinstein et al., 2015). At the cellular level, sources include electrical noise, thermal agitation, channel noise, neural adaptation, and synaptic plasticity (Clifford et al., 2007; Faisal et al., 2008; Feldman, 2009; Manwani & Koch, 1999). At the network level, random fluctuations arise from homeostatic adjustments to excitation/inhibition balance, changes in attention and arousal, interactions among large neural populations, and modulation of inter-regional connections (Clare Kelly et al., 2008; Fontanini & Katz, 2008; Turrigiano, 2011; van den Brink et al., 2019). These combined mechanisms (and others) may generate substantial variability both at rest and across trials during a task performance (Baracchini et al., 2021; Uddin, 2020).

A few studies have investigated the combined influence of external and neural noise in eliciting SR-like phenomena and found that that external and neural noise could synergistically enhance sensory and cognitive functions. Kitajo et al., (2003, 2007) found that introducing visual noise to one eye could improve visual signal detection in the other, an effect correlated with increased brain-wide phase synchronization. Aihara et al. (2008) explored visual detection in the presence and absence of visual noise, defining indices to measure external stochastic resonance effects and their correlation with internal noise levels, which was supported further by computational models (Aihara et al., 2010).

Recent research has shifted toward modulating internal neural noise through electrical stimulation rather than external noise sources. This research includes studies by Battaglini et al. (2023), Pavan et al. (2019), and van der Groen et al., (2018; 2016), who employed noninvasive transcranial random noise stimulation (tRNS) to modulate neural noise in targeted brain areas responsible for visual processing.

In addition to immediate changes, neural noise is subject to long-term changes that take place throughout life. In the process of healthy aging, the brain undergoes gradual structural changes while maintaining a high level of cognitive ability, in the sense that these changes often are accompanied by a reorganization of functional brain networks (Reuter-Lorenz & Park, 2014). Various neurocognitive theories of aging have debated whether such changes are advantageous or detrimental. Some argue that age-related changes are due to the combined effects of age-related structural changes and the change in the dynamics of a metastable system (Naik et al., 2017).

The neural noise hypothesis of aging suggests that owing to age-related increased neural noise, the signal-to-noise ratio (SNR) of the central nervous system degrades during aging, which leads to diminished cognitive performance (Cremer & Zeef, 1987; Li et al., 2001; Welford, 1981). In support of this hypothesis, Voytek et al. (2015) have measured with EEG the within-population spiking asynchrony and the local field potential 1/f slope. They observed an age-related flattening in the EEG 1/f slope, which means a higher level of 1/f noise. These changes have been associated with cognitive decline, specifically with working memory (Voytek et al., 2015). Further findings confirmed that with age there is a notable flattening of the 1/f exponent, indicative of an increase in local asynchronous activity in the cortex (Cesnaite et al., 2023; Clark et al., 2024; Dave et al., 2018; Finley et al., 2024; Merkin et al., 2023; Pathania et al., 2022; Tran et al., 2020; Voytek et al., 2015; Waschke et al., 2017), which is associated with cognitive decline in specific areas, such as working memory (Thuwal et al., 2021; Voytek et al., 2015), speeded processing (Pathania et al., 2022), and visual spatial attention (Tran et al., 2020).

Another line of research has instead suggested that aging is associated with a reduction in neural noise, reporting a decrease in trial-to-trial variability in BOLD responses and a consequent behavioural decline (Garrett et al., 2011). Variability has been demonstrated to convey task-related information in animal models (Denfield et al., 2018; Scaglione et al., 2011) and in human studies (Burlingham et al., 2022; Dinstein et al., 2015). In this sense, neural variability is a positive, not negative, factor (Waschke et al., 2021), indicative of neural adaptability to tasks (Nomi et al., 2017). Beyond the conceptualization of variability as noise, a deeper analysis of Garrett's results (2011) reveals that only some brain areas have been found to show less variability in older people. In contrast, other areas have shown the opposite pattern. Moreover, a key finding was that the pattern of variability in the aged brain was more diffuse. This last finding can be not a hallmark of a reduction in neural noise, but can result from age-related dedifferentiation. Furthermore, measuring EEG activity, P300 latencies (reflecting cognitive functions) appeared to be more variable with age (Kilgler et al., 1993). However, variability in BOLD and EEG signals at rest relates differently to aging in the human brain (Kumral et al., 2020), partially owing to the different temporal resolutions of these tools. Given the temporal resolution, fMRI signal fluctuations are the result of time integration of activation across large neural populations and therefore are indices of network-level variability connected to structural brain connectivity (Baracchini et al., 2021; Fallon et al., 2020). Although EEG predominantly reflects oscillatory activities, it also is influenced by microscale neurophysiological factors; aperiodic neural activity can generate detectable scalp potentials and shape broadband EEG features (Brake et al., 2024). Background aperiodic or "scale-free" broadband activity is present across all frequencies, adhering to a  $1/f$  power distribution where spectral power decreases with increasing frequency (Pritchard, 1992), constituting a large proportion of the spontaneous neural activity recorded from the cortex (He et al., 2010).  $1/f$  spectral exponent has been shown to track variations in the balance of excitation and inhibition (E/I; Gao et al., 2017), which in turn is closely linked to neural variability on fine timescales (Harris & Thiele, 2011; Kanashiro et al., 2017). Therefore, it is important to note that the choice and interpretation of variability measures strongly affect the direction of observed effects (Waschke et al., 2021).

Mechanistically, increased neural noise is attributed to a dysregulation of homeostatic protective mechanisms in late adulthood, altering the inhibition/excitation balance (Radulescu et al., 2023). Ageing induces an increase in excitatory signalling (Rozycka & Liguz-Leczna, 2017), causing an E/I imbalance, which then increases internal noise levels (Bennett et al., 2007; Casco et al., 2017; Cremer & Zeef, 1987;

Hua et al., 2006; Tran et al., 2020; Voytek et al., 2015; Welford, 1981), primarily due to a reduction of GABA (Chamberlain et al., 2021; Hickmott & Dinse, 2012; Leventhal et al., 2003). In addition to the neurochemical alterations, the SNR during visual perceptual processing in the senescent brain is compromised by a reduction in structural integrity that triggers compensatory mechanisms in aged visual circuits (Parvez et al., 2021; Silva et al., 2020). As a result, the effectiveness/occurrence of SR in the elderly might be altered (Li et al., 2006). In our study, we define neural noise as the asynchronous, randomly generated brain activity that constitutes the aperiodic component of the EEG spectrum. Because the optimal functioning of SR requires an optimal overall sum of internal and external noise, alterations in internal noise levels necessitate adjustments to external noise to maintain the appropriate overall noise level (Aihara et al., 2008; Yi et al., 2006; Zhang et al., 2017).

A recent study by Battaglini et al. (2023) supports this interpretation. They stimulated the cortex of healthy adults with a noninvasive neuromodulatory technique based on an alternating current with randomly varying intensity (tRNS), which was supposed to modulate the amount of neural noise. Participants performed a coherent motion detection task in which external noise was manipulated by varying the total number of dots. Results showed that neuromodulation induced by tRNS caused a leftward shift in the peak of performance when accuracy was plotted as a function of external noise (dots numerosity). More specifically, when 1 mA-tRNS was applied to increase neural noise, the peak in performance was obtained for a lower level of external noise. This result suggests an inverse relationship between the amount of neural and external noise required to reach the threshold, and hence SR. In contrast, the results of the previous computational study by Li et al. (2006) suggested a direct relationship between the amount of neural<sup>1</sup> and external noise required for optimal SR. In their study, a stochastic gain-tuning model was used to simulate changes in SR in the senescent brain. They reproduced the age-related increase in endogenous noise by changing the gain parameter (G) in the model. In doing so, they demonstrated that cognitive aging, characterized by heightened intrinsic neuronal noise but diminished plasticity, necessitates an increased amount of external noise for the SR phenomenon to manifest. This was illustrated by a consistent shift in peak performance towards higher levels of external noise, i.e., to the right in the inverted U-shaped curve (Li et al., 2006).

Given the conflicting evidence in the literature, understanding how age-related increases in neural noise impact the strength and occurrence of SR throughout the lifespan

<sup>1</sup> Neural noise is called internal noise in Li et al. (2006).

remains unclear. In our study, we aimed to test the predictions of Li et al. (2006) model by using psychophysical methods, focusing on age-related changes in SR within the adult visual system.

Motion perception is an ideal model for studying perceptual aging (Billino & Pilz, 2019). We employed the Random-Dot Kinematogram (RDK) task, where participants detect coherent motion amidst randomly moving dots. This task requires integrating multiple motion signals for accurate detection. Ho and Giaschi (2009) demonstrated that both low- and high-level versions of first-order RDKs activate motion-sensitive areas, such as MT, indicating their role in processing varying complexities of motion information. Moreover, coherence perception correlates directly with activity levels in the motion-sensitive middle temporal area MT. Previous studies have shown that age-related changes impact both motion perception thresholds and activity in motion-sensitive brain regions (Biehl et al., 2017; Ward et al., 2018).

Our study involved a group of healthy adults spanning an age range from 18 to 82 years, all of whom engaged in a two-interval forced-choice task. Participants were required to determine which of two successive displays contained coherent motion. This setup allowed us to explore age-related changes in SR using two distinct experimental blocks, each with specific manipulations. In the initial block, we manipulated the coherence level of the stimuli. Coherence level in this context refers to the ratio of dots moving coherently in a specified direction (e.g., rightward) to the total number of dots presented. In contrast, the second block kept coherence level constant while varying dot density. This manipulation involved adjusting the total number of dots within the same spatial area of the display, thereby increasing perceptual noise in the stimulus.

Stochastic resonance occurs with stimuli close to the perceptual threshold. The initial block also served to calibrate task difficulty through an adaptive procedure, aiming for 70.7% accuracy based on individual coherence thresholds. By standardizing task difficulty across participants in this way, we could later isolate the effects of external noise (dot density) on SR from individual differences in coherence thresholds.

It is crucial to distinguish between manipulating dot density and manipulating coherence level or SNR, typically defined as the ratio of coherent dots moving rightward to randomly moving dots. Increasing dot density introduces Correspondence Noise, stemming from uncertainties in matching dots across frames, which may mask coherent motion (Barlow & Tripathy, 1997; Tripathy et al., 2012). A large increase in density not only activates occipital areas more but also tends to reduce task accuracy (Ho & Giaschi, 2009; Tripathy et al., 2012). We expect increased external noise due to increased density to interact with internal noise.

In both blocks, the coherent dots were consistently present on one of the two screens per trial, although participants often erred. An incorrect response indicates that the coherent dot signal failed to exceed the participant's detection threshold. Adding noise (increasing density) that results in fewer errors (increased accuracy) implies that the noise raised the signal above the detection threshold by enhancing detector aggregation (integrative mechanisms). Conversely, if performance deteriorates, it suggests that the noise has likely overwhelmed the signal, consistent with the “classical” threshold SR paradigm.

Participants in the thresholding block were randomly assigned to two subgroups tested with different dot numbers (100 vs. 400 dots). This division served dual purposes. First, it ensured that participants did not exhibit better performance in the second block under the same density conditions as in the first block due to practice effects. By employing two densities for the staircase, we could detect an eventual bimodal distribution in the second block indicative of practice effects, independent of age. Second, it enabled us to explore the impact of density on coherence level thresholds across different age groups by comparing the slope of age-related threshold regressions between the 100-dot and 400-dot groups.

In the thresholding block, we expected a general age-related deterioration in performance and better thresholds in the condition with fewer dots (less external noise) for older adults (Hutchinson et al., 2014). For SR in the constant stimuli block, we expected to observe the typical peak at intermediate levels of external noise in young adults and a flattening of the curve with aging (Li et al., 2006). Regarding the positioning of the peak with respect to the amount of noise, we hypothesized two possible outcomes: 1) as age increases, the peak shifts to the left, i.e., inverse relationship between neural and external noise (Battaglini et al., 2023); and 2) as age increases, the peak shifts to the right, i.e., direct relationship between neural and external noise (Li et al., 2006).

## Methods

### Participants

A total of 286 participants took part in the experiment, all possessing normal or corrected-to-normal vision. The mean age of the participants was 45.92 years ( $SD = 19.85$ ). Before the commencement of the study, three exclusion criteria were established:

- 1) Participants with a coherent motion threshold above 75% in the initial block staircase were excluded (32 participants).

- 2) Participants who did not achieve a minimum of 6 reversals in the last 40 trials of the first block, which is necessary to ensure accurate threshold estimation, were excluded (5 participants).
- 3) Participants with an average percentage of correct responses exceeding 90% in the second block were excluded to avoid ceiling effects (28 participants).

After applying these exclusion criteria, 214 participants remained for subsequent analysis. This final sample included 92 females and had a mean age of 43.52 years ( $SD = 19.61$ ), with the age range spanning from 18 to 82 years. The age distribution of the final sample is depicted in Fig. 1.

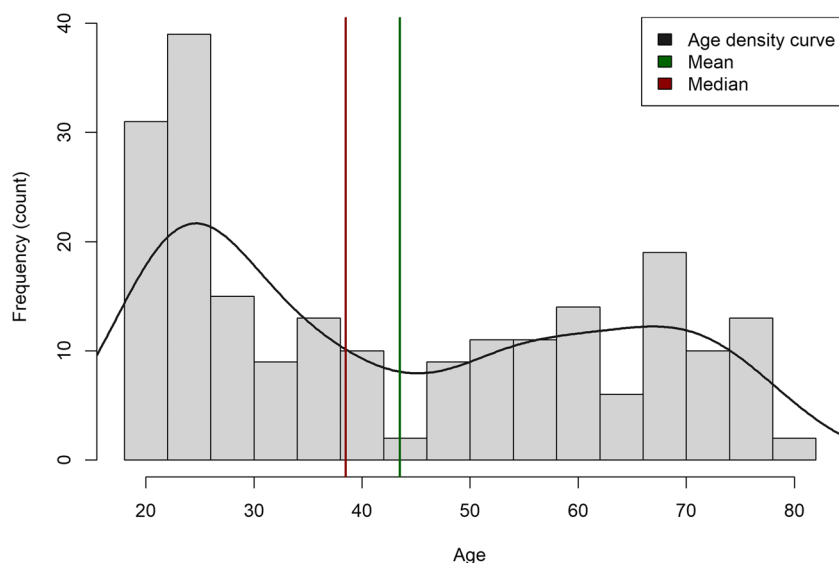
The Ethics Committee of Psychological Research (Area 17) at the University of Padova granted approval for the experiment (protocol 4014). The procedures employed in this study align with the principles outlined in the Declaration of Helsinki. Before data collection, all participants provided informed consent for both participation in the study and the publication of anonymized aggregated data.

## Apparatus and stimuli

Participants performed the task on their own computer, remotely via the internet. At the beginning of the experiment, they were asked to sit in a quiet, semidark room, with no direct light on the screen. The task was implemented using HTML (Hyper Text Markup Language), CSS (Cascading Style Sheets) and jsPsych, an open-source JavaScript library developed specifically as a framework for web-based psychological experiments (de Leeuw, 2015). The

experiment was hosted on a server located at the Department of General Psychology at the university of Padova and was made available online thanks to a JATOS instance (Lange et al., 2015). Participants were recruited among the acquaintances of the experimenters' collaborators and were unaware of the goals of the study. Each participant received the link for participation in the experiment via email together with a copy of the informed consent. A computer with a screen size of at least 10 in. was required for participation. People with touchscreen devices, such as smartphones and tablets, were excluded from participation. Participants were also asked to maintain a viewing distance of 57 cm from the screen, with the monitor perpendicular to the line of gaze throughout the experiment. The first screen presented participants with an informed consent form, before continuing. In a second screen, after entering some information (age, gender, and handedness), participants were asked the size of the monitor in centimetres. Based on the size of the monitor and resolution, we then calculated the individual number of pixels per degree of visual angle. Subsequently, all visual elements in the experiment were scaled according to this number to ensure consistency of stimulus size between participants.

The Random Dot Kinematogram (RDK) is a stimulus widely used in motion studies both in lab and online (Rajananda et al., 2018). In RDKs, a certain percentage of dots are designated to move in one coherent direction, and the remaining percentage of dots are designated to move in random directions. In this experiment, coherent dots moved in the direction of coherent motion in all frames, contrary to random dots. The direction of the coherently moving dots was rightward; the other dots moved to an adjacent position



**Fig. 1** Frequency distribution of the age of the participants. Histogram represents the frequency distribution of age in the dataset, with a density curve (grey line) overlaid. Green line indicates the mean

age, while the red line represents the median age. Bin width for the histogram is set to 4 units. The plot provides insights into the central tendency and distribution of age in the examined population

in a random direction in each frame (“random walk”). The stimuli consisted of white dots moving on a black background (Fig. 2). The aperture was a square window of  $10^\circ$ , displayed at the centre of the screen while dot diameter was  $0.075^\circ$ . In each frame, dot displacement was  $0.05^\circ$ , resulting in a speed of 3 deg/s. The “dot lifespan,” which determines the time that pass before a dot disappears and reappears somewhere else within the aperture, was set to be longer than the stimulus duration. If a dot reached the end of the squared aperture, they were then reallocated to a random point on the opposite edge. Stimuli were created by means of the RDK jsPsych plugin (Rajananda et al., 2018).

## Procedure

The motion detection task used a two-interval forced-choice paradigm and was mutated from two previous laboratory studies in which an inverted U-shaped curve for performance as a function of dots numerosity was found (Battaglini et al., 2020, 2023). Participants decided which of two sequentially presented RDKs displayed a more coherent rightward direction of motion (Fig. 3).

The experiment comprised two blocks: a thresholding block and a constant stimuli block. Each of these blocks was preceded by a 10-trial practice session.

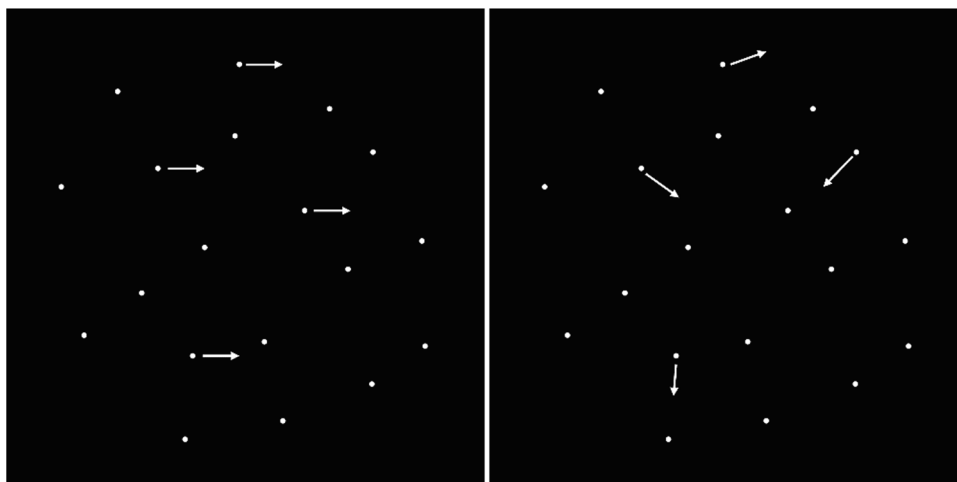
In the initial thresholding block, the total number of dots remained constant, while the proportion of coherently moving dots varied using a one-up two-down Levitt staircase (Levitt, 1971). Participants in this block were randomly assigned to one of two subgroups. One subgroup ( $N = 118$ , mean age = 43.18) had an initial threshold determined with a numerosity of 100 dots; the other subgroup ( $N = 96$ , mean age = 43.94) had a numerosity of 400 dots.

In the staircase procedure, the initial coherence level was set at 70%, and the initial step size was set at 10%. Following each reversal, the step size progressively decreased by 5%, 3%, 2%, and ultimately 1%. The staircase concluded after 12 reversals, and the threshold was computed as the average of the reversals, excluding the initial 4. This average denoted the minimum coherence level required for observers to accurately detect rightward motion 70.7% of the time.

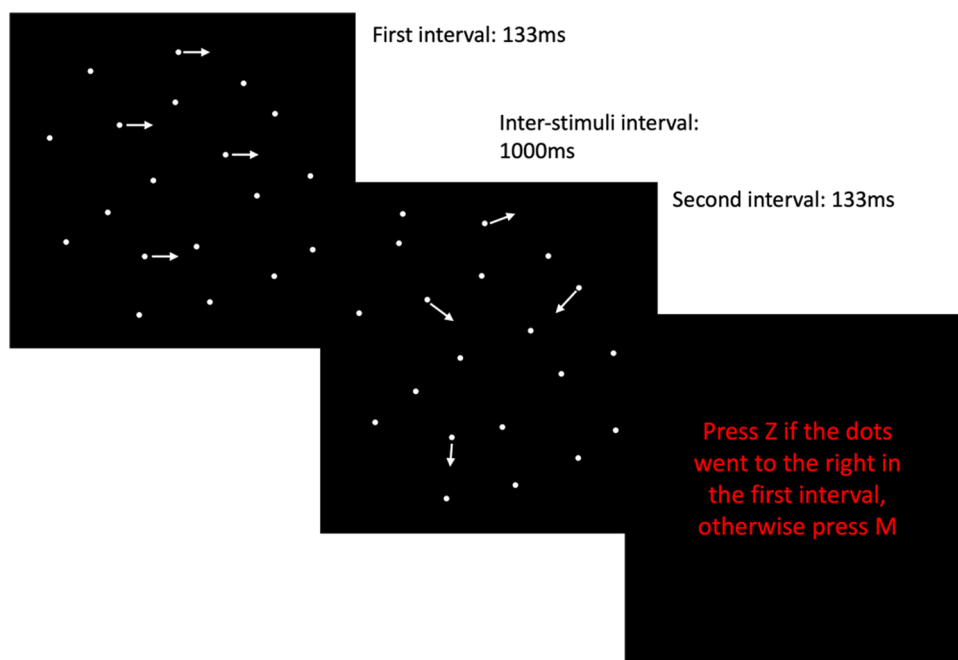
Instructions were repeated before each trial, and feedback on response accuracy was provided. Each trial commenced with a fixation cross displayed for 1000 ms in red with a visual angle of half a degree. Subsequently, the first RDK was presented, followed by a 1000-ms poststimulus gap, and then the second RDK. Another 1000-ms poststimulus gap preceded participant response. A 100-ms warning sound preceded the presentation of both RDKs.

In each trial, a standard RDK consisted of randomly moving dots, alongside a target RDK containing a few coherent rightward moving dots (Fig. 3). Participants were instructed to press the “z” button if the target was in the first interval or the “m” button if in the second interval. Responses were recorded after both intervals were presented, and the subsequent trial began automatically upon pressing the response key. A red circle in experimental trials signalled when participants should respond.

The second block was identical to the first except for the change in the procedure from adaptive to constant stimuli. The random-to-coherent dots ratio was set based on the threshold obtained from the first block. In alignment with the methodology of Battaglini et al. (2023), the overall number of dots varied across 14 levels, strategically selected along a quasi-logarithmic scale (20, 29, 41, 58, 83, 118, 168, 239, 340, 485, 691, 999, 1403, and 2000 dots). The decision to adopt a logarithmic spacing was influenced by



**Fig. 2** Statically, two examples of the configuration of moving dots presented throughout the experiment. A configuration of moving dots with a percentage of coherently moving dots (left). All the dots move randomly (right)



**Fig. 3** Trial sequence consisted of a 133-ms initial interval featuring coherent (or random) motion, followed by a 1000-ms post-stimulus gap. Subsequently, there was a second 133-ms interval with random (or coherent) motion, another 1000-ms poststimulus gap and, finally, the participant's response. During the practice block, the

response was followed by visual feedback. Trial-by-trial instructions were exclusively presented during practice trials. In the experimental trials, a red circle replaced the instructions, signalling participants when to provide their response

the understanding that the perception of motion and point numerosity adheres to a compressive nonlinearity, akin to Weber's Law (Zanker, 1995). Each of these 14 levels comprised 20 trials, resulting in a total of 280 pseudorandomized trials. Accuracy, defined as the proportion of correct responses at each noise level, was measured.

### Data analysis

We utilized the statistical software R (R Core Team, 2013) to conduct analyses and create figures. For the statistical analyses, continuous variables were first scaled and centered using the “scale()” function in R.

In the first experimental block, our objective was to investigate the effects of dot density and age on coherence level thresholds. For this purpose, we employed a linear model with the natural logarithm ( $\ln$ ) of the threshold as the dependent variable. Coherence level thresholds are defined as the ratio of dots moving coherently in a specified direction (e.g., rightward) to the total number of dots presented, expressed as a percentage. The dependent variable ranged as an integer from 0 to 100, representing the percentage of coherent dots.

The choice of  $\ln$  transformation aimed to capture the observed compressive nonlinearity in dot numerosity and motion perception (Zanker, 1995). This decision was

reinforced by a substantial enhancement in the distribution of model residuals after the transformation. The model included the participant's age as a continuous predictor and group as a two-level factor, representing the number of dots in the staircase procedure (either 100 or 400 dots). We assessed the significance of factors using an F-test.

For the examination of SR in the constant stimuli block, we employed a generalized linear mixed model with the binomial variable accuracy as the dependent variable. The model included the participant's age and the logarithm of the number of dots as continuous predictors. To address within-subject correlation in repeated measures, the model featured an individual random intercept. Regarding the number of dots, we hypothesized a nonlinear effect, resulting in an inverted U-shaped curve. Model selection involved comparing four mixed models, estimated using the `glmer()` function from the “lme4” package (Bates et al., 2019) in R. The number of dots variable was modelled with linear regression in one model and subsequently with polynomials up to the fourth degree. Orthogonal polynomials for the SOA variable were calculated using the `poly()` function in R.

We selected the best model based on the Akaike information criterion corrected for small sample sizes (AICC) with the `aictab()` function from the “AICcmodavg” package (Mazerolle, 2023). This test determined whether a non-monotonic (curve) model outperformed a linear one. After

choosing the best model, we conducted an omnibus test to assess significance, utilizing a Type III Wald chi-square tests with the Anova() function from the “CAR” package (Fox & Weisberg, 2019).

Given that the age distribution of participants (refer to Fig. 1) was nonuniform, during the review process, we accommodated a suggestion to incorporate a statistical test that would explore the effect of age as a binary factor rather than as a continuous variable. To implement this, we partitioned the sample into two age-based groups—“younger” individuals ranging from 18 to 50 years, and “older” individuals from 50 to 82 years, each spanning 32 years. Consequently, we adapted the previously selected optimal model by replacing the continuous age variable with a categorical variable representing these age groups. On this modified model, we again applied an omnibus test to assess significance using a Type III F-test with the Satterthwaite approximation for degrees of freedom.

We assessed model assumptions using the DHARMA R package (Hartig & Lohse, 2022). This package employs a simulation-based method to examine residuals for fitted Generalized Linear Mixed Models (GLMMs). The Asymptotic one-sample Kolmogorov–Smirnov test identified a significant deviation from the expected distribution for both the linear thresholding model ( $D=0.05$ ,  $p<0.001$ ) and the constant stimuli linear mixed model with both continuous ( $D=0.033$ ,  $p=0.003$ ) and categorical age ( $D=0.032$ ,  $p=0.005$ ). Upon visual inspection, this deviation appears negligible. Importantly, neither the dispersion test nor the outlier test yielded significant results. Therefore, in the absence of clear signs of heteroscedasticity or over/under dispersion, we proceeded with the analyses using these models.

For the LMM in the thresholding block results were reported using the “report” package (Makowski et al., 2020), and effect sizes were labelled following Field’s recommendations (Field, 2013). For the GLMM in the constant stimuli block as an estimate of the effect size, we calculated the semi-partial coefficients of determination, also known as part $R^2$  ( $\Delta R^2$ ), by means of the partR2 package (Stoffel et al., 2021). As suggested by Stoffel, part R2 for main effects and interactions were calculated separately and part R2 for the main effects were estimated after excluding the interaction from the model.

## Results

In the initial experimental phase, we investigated the variation in performance, which we defined as the logarithm of the number of dots required to identify the interval with coherent motion 70.7% of the times. This exploration focused on the threshold for two levels of dot numerosity, specifically 100 and 400 (representing external

noise), in relation to age. Figure 4 visually represents the  $\ln(\text{threshold})$  as a function of participants’ ages at two levels of dot numerosity.

The results, assessed through an F test, indicated a statistically significant yet small main effect of staircase dot numerosity ( $F(1, 2992) = 33.04$ ,  $p < 0.001$ ; partial  $\eta^2 = 0.01$ , 95% CI [5.58e-03, 1.00]). The estimated marginal mean for the staircase with 100 dots was 2.88 (standard error = 0.021, degrees of freedom = 2992, CI [2.84, 2.92]), equivalent to 17.8 dots. In contrast, the estimated marginal mean for the staircase with 400 dots was 2.69 (standard error = 0.036, degrees of freedom = 2882, CI [2.64, 2.74]), equivalent to 14.7 dots.

The main effect of age was also statistically significant, though small ( $F(1, 2992) = 141.74$ ,  $p < 0.001$ ; Partial  $\eta^2 = 0.05$ , 95% CI [0.03, 1.00]). With each passing year, there was an observed increase in the threshold of 0.192 on a logarithmic scale, equivalent to 1.21 dots.

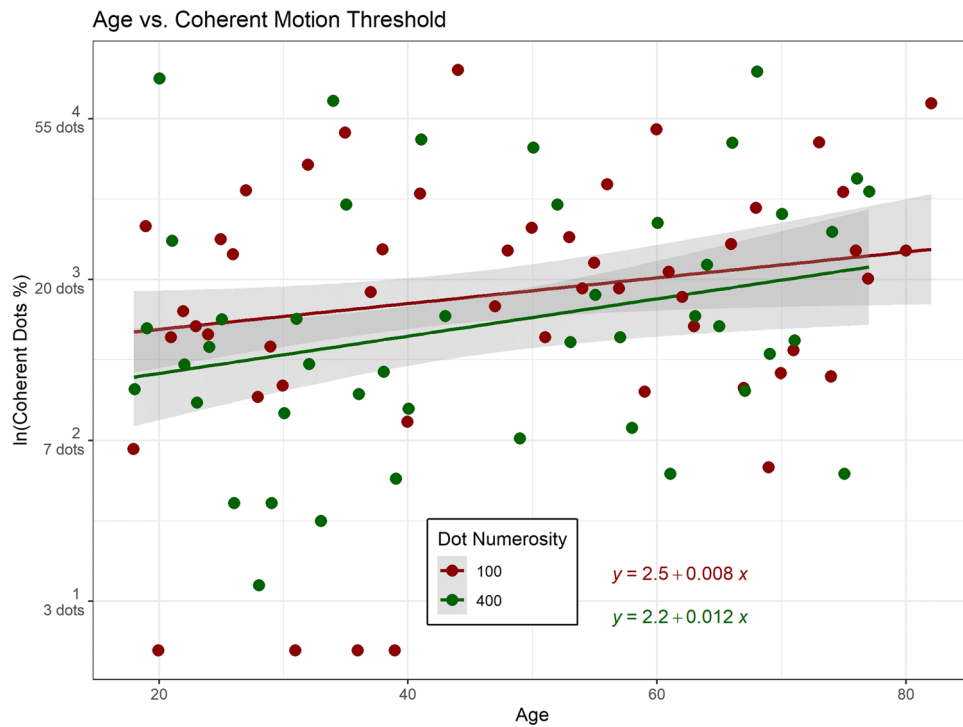
Furthermore, the interaction between staircase dot numerosity and age was statistically significant, with a very small effect size ( $F(1, 2992) = 4.89$ ,  $p = 0.027$ ; Partial  $\eta^2 = 1.63e-03$ , 95% CI [9.59e-05, 1.00]). For each year of age, the difference between the staircase with 100 dots and the one with 400 dots decreased by  $-0.035$  on a logarithmic scale, equivalent to  $-0.96$  dots.

When examining the relationship between performance and dot numerosity (Fig. 5), a peak was observed at intermediate levels. Visual exploration data were supported by model selection, where the model incorporating dot numerosity as a fourth-degree predictor outperformed other models (AICcWt = 0.64), particularly surpassing the linear dot numerosity model (AICcWt = 0). Comprehensive results of the model selection are presented in Table 1.

The marginal  $R^2$  and 95% CI for the full model were  $R^2 = 0.01$ , 95% CI [0.01, 0.013]. The omnibus Type III Wald chi-square test over the best model (fourth degree) suggested that the main effect of the logarithm of the number of dots was statistically significant and substantial, explaining a significant portion of the model’s variance ( $\chi^2(4) = 611.2400$ ,  $p < 0.001$ ;  $\Delta R^2 = 0.01$ , 95% CI [0.008, 0.012]). The main effect of age was statistically not significant and very small ( $\chi^2(1) = 0.4579$ ,  $p = 0.499$ ;  $\Delta R^2 = 0.0002$ , 95% CI [0, 0.002]). The interaction between the logarithm of the number of dots and age was statistically significant and very small ( $\chi^2(4) = 28.7636$ ,  $p < 0.001$ ;  $\Delta R^2 = 0.0004$ , 95% CI [0, 0.001]).

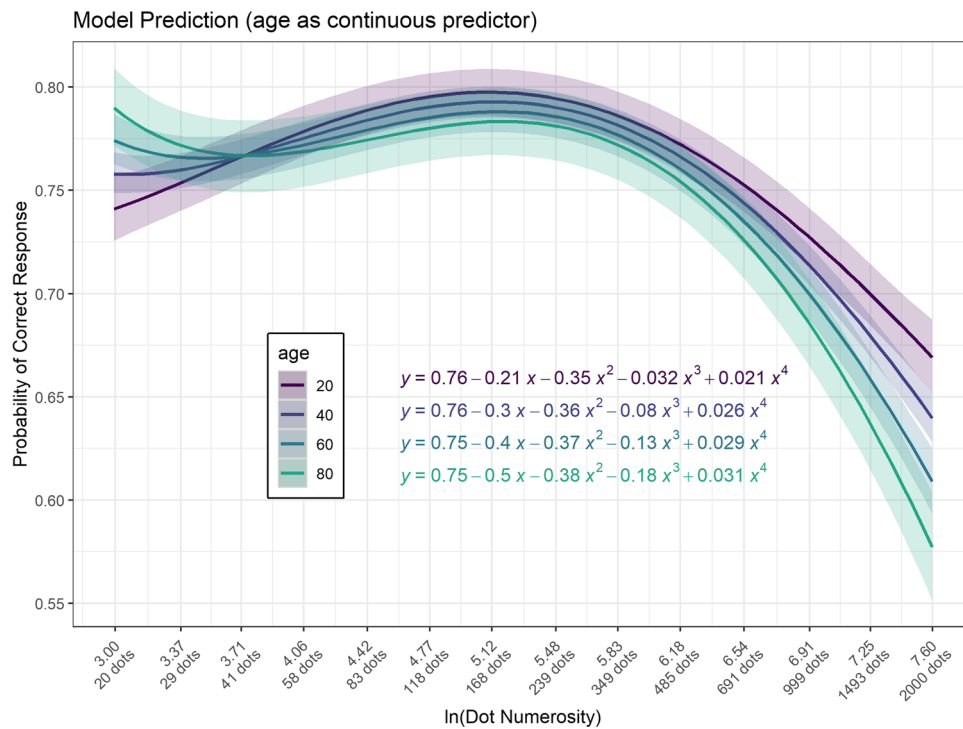
Figure 5 illustrates the predictions generated by the fourth-degree model. Despite entering the age variable as a continuous parameter in the model, we opted to visually represent it across four distinct age levels. The model’s prediction for an individual aged 20 years is expressed by the equation  $Y = 0.76 - 0.21x - 0.35x^2 - 0.032x^3 + 0.021x^4$ , while for an 80-year-old individual, it is given by  $Y = 0.75 - 0.5x - 0.38x^2 - 0.18x^3 + 0.031x^4$ . It is





**Fig. 4** Age-related changes in threshold for coherent RDK. The plot shows how the ln(threshold) for detecting coherent motion, expressed as the natural logarithm of the percentage of coherent dots out of the total dots, varies with age for staircases with 100 and 400

dots. Linear regression lines, shaded 95% confidence bands, and individual data points are included. Red line corresponds to the staircase with 100 dots. Green line represents the staircase with 400 dots



**Fig. 5** The relationship between accuracy, dot numerosity, and age. Lines represent predictions of the fourth-degree model. Although the age variable in the model is inherently continuous, for

visualization, we have represented it through four age levels. The x-axis represents dot numerosity on a logarithmic scale. The coloured bands represent the 95% confidence intervals

**Table 1** Model selection based on AICc

Model	K	AICc	Delta AICc	AICcWt	Cum.Wt	LL
Fourth degree	11	13,408.62	0.00	0.64	0.64	−6693.26
Cubic	9	13,409.76	1.14	0.36	1.00	−6695.85
Quadratic	7	13,424.48	15.87	0.00	1.00	−6705.22
Linear	5	13,720.58	311.96	0.00	1.00	−6855.28

K=number of parameters in each model; AICc=Akaike Information Criterion corrected for small sample sizes; Delta AICc=difference in AICc values between each model and the best-fitting model; AICcWt=Akaike weight, representing the likelihood of each model being the best-fitting model; Cum.Wt=cumulative weight, the sum of AICc weights up to the current model; LL=log-likelihood, a measure of how well the model explains the observed data

noteworthy that with increasing age, there is a gradual augmentation in the negativity of both the linear and cubic terms. This interaction results in a flattening of the curve for lower dot numerosity values (left side of the curve) and a sharp decline in performance for higher dot numerosity (right side of the curve).

When analysing age as a dichotomous variable, the participants were divided into two age-defined groups: the younger group comprised 123 individuals within an age range of 18 to 50 years, and the older group included 91 individuals aged between 50 and 82 years. The marginal  $R^2$  and 95% CI for the full model were  $R^2=0.01$ , 95% CI [0.01, 0.013]. The omnibus Type III Wald chi-square test indicated that the main effect of the logarithm of dot numerosity was statistically significant and substantial, explaining a significant portion of the model's variance ( $\chi^2(4)=630.848$ ,  $p<0.001$ ;  $\Delta R^2=0.01$ , 95% CI [0.008, 0.011]). Conversely, the main effect of age group did not reach statistical significance and had a negligible effect size ( $\chi^2(1)=0.504$ ,  $p=0.478$ ;  $\Delta R^2=0$ , 95% CI [0, 0.001]). However, the interaction between the logarithm of dot numerosity and age group was statistically significant, albeit small ( $\chi^2(3)=38.031$ ,  $p<0.001$ ;  $\Delta R^2=0.001$ , 95% CI [0, 0.003]). The predictive model for the younger group was described by the equation  $Y = 0.76 - 0.22x - 0.36 - 0.047x^3 + 0.026x^4$ , while for the older group, it was articulated as  $Y = 0.75 - 0.45x - 0.37x^2 - 0.15x^3 + 0.025x^4$ . The results further demonstrated an increase in the negative coefficients of linear and cubic terms with for the older age group, thus corroborating the findings obtained when age was modelled as a continuous variable. Figure 6 illustrates the predictions generated by the fourth-degree model with age group as a categorical two-level factor.

## Discussion

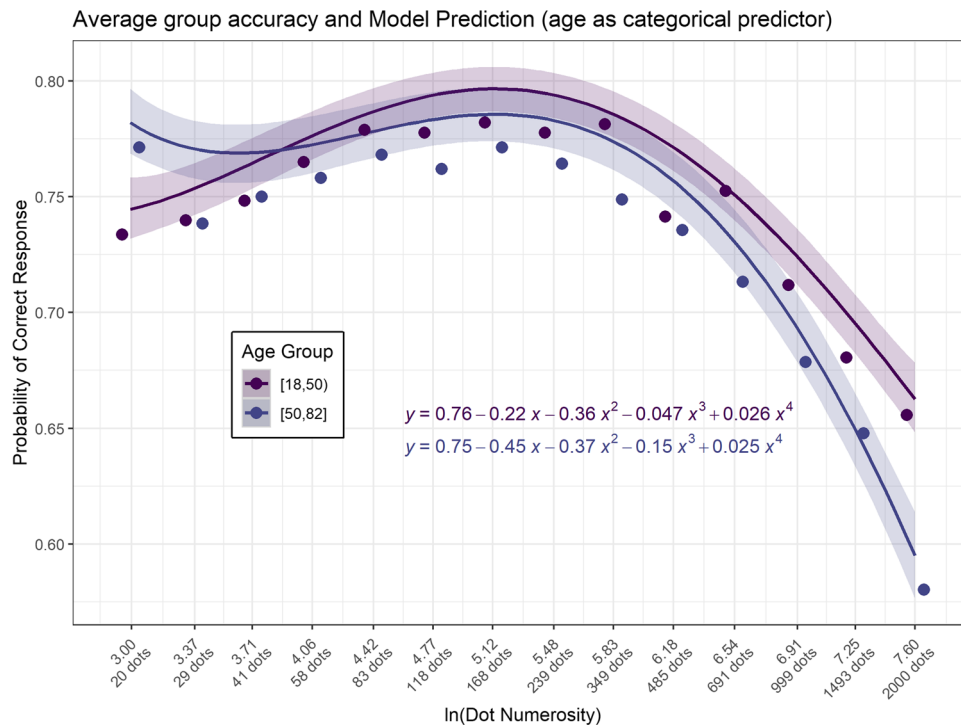
The purpose of the study was to investigate age-related changes in psychophysical stochastic resonance (SR) within human visual perception, considering external noise as a

variable. A sample of healthy adults underwent a two-intervals forced-choice coherent motion discrimination task with RDK stimuli. Two separate blocks were administered. In the first, we determined the coherence level required for a 70.7% accuracy performance. In the second, using a constant stimulus procedure, we manipulated external noise (total dot number) to assess its impact on accuracy.

As expected, initial thresholding block indicated a decline in coherent motion detection ability with increasing participant age, aligning with findings from previous studies (Braham Chaouche et al., 2020; Pilz et al., 2017; Trick & Silverman, 1991) showing age-related deterioration in global motion perception. Coherent motion detection involves pooling similar motion signals while suppressing irrelevant ones (Dakin et al., 2005). This decline in ability may be attributed to increased tonic neural noise negatively affecting stimulus-associated neural variability in aging (Tran et al., 2020). Interestingly, younger participants demonstrated improved performance with more dots (400), whereas this advantage diminished for older adults. Higher dot numerosity theoretically facilitates global pooling by increasing the likelihood of combining motion signals from the target direction (Dakin et al., 2005). However, for older adults, the detrimental impact of increased global noise may outweigh the benefits of enhanced pooling.

Our results parallel findings by Hutchinson et al. (2014). In their investigation, they assessed the performance of both young and old participants under three distinct conditions: equal dot numbers but varied sizes and densities (exp. 1); uniform density but increased dot number and size (exp. 2); uniform size but heightened density and dot number (exp. 3). In contrast to younger participants, elderly participants in both Experiments 1 and 2 did not demonstrate improved performance as the dot number or size increased. However, in Experiment 3, mirroring our initial experimental phase, no statistically significant difference in performance between young and old participants was observed.

Despite the lack of statistical significance, a closer examination of the data revealed a notable trend—an inverse relationship between density and performance for both



**Fig. 6** The relationship between accuracy, dot numerosity, and age group as a categorical two-level factor. Dots represent average accuracy for each group. Lines depict the predictions of the fourth-

degree model. X-axis denotes dot numerosity on a logarithmic scale. Coloured bands represent the 95% confidence intervals

age groups. Young individuals excelled at high density, whereas older individuals exhibited better performance at low density. This observed trend in Hutchinson et al. (2014) is in agreement with our results in the thresholding block. The difference in statistical outcome may be attributed to a large difference in statistical power between the two studies ( $N=18$  in Hutchinson et al. compared with our  $N=214$ ). By integrating our results with prior research, we posit that in an aging neural system characterized by heightened intrinsic noise, performance is hindered rather than improved by increased dot number/density, unlike in younger individuals.

Following the standardization of baseline performance, we further examined the influence of advancing age on SR. Employing the constant stimulus method, we systematically varied the total number of dots from 20 to 2000 while maintaining a consistent stimulus size. Performance was then assessed across 14 levels of dot numerosity. As anticipated, the accuracy plotted against dot number exhibited the characteristic inverted U-shaped curve associated with SR (Battaglini et al., 2023).

This result was corroborated by model selection, wherein polynomial models of second degree and higher outperformed the linear model. The model offering the best balance between fit and parsimony, as determined by the AICc, was the fourth-degree polynomial model. However, the difference in AICc between the fourth-degree model and

the cubic model was less than 2, indicating that both models were nearly equivalent, with a slight preference for the fourth-degree model owing to the decrease in log-likelihood (Arnold, 2010). Notably, the fourth-degree term exhibited minor age-related differences, whereas significant differences were observed in the linear and cubic terms, which became increasingly negative with advancing age.

According to the predictions of the fourth-degree model, as age increases, the curve becomes less steep to the left of the peak and steeper to the right. Surprisingly, in the oldest individuals (around 80 years of age), optimal performance was observed at the lowest external noise level (peak shifted to the left), with accuracy declining as the number of dots increased. This differs from the beneficial SR effect observed in younger participants. These findings suggest that with advancing age and increased neural noise, the sweet point for optimal performance shifts towards lower external noise levels.

Concerning our initial hypothesis, whereas the flattened curve in the elderly aligns with predictions from Li & colleagues (2006), the leftward shift of optimal performance does not. Instead, it aligns with the findings of Battaglini et al. (2023). For younger adults, the addition of weak external noise may not surpass the threshold, resulting in suboptimal performance. Conversely, in the brains of older adults, the weak external noise combines with an elevated level of

internal noise, potentially triggering SR. When external noise is optimized for inducing SR in younger individuals, performance deterioration is observed in older individuals.

The addition of an optimal level of external noise has been demonstrated to amplify responsiveness to visual stimuli by boosting the neuronal firing rate (Srebro & Malladi, 1999). However, in the elderly, the baseline noise in the visual cortex is already high (Talyansky & Brinkman, 2021; Tran et al., 2020; Yan et al., 2020). Consequently, lower amounts of external noise may be sufficient to trigger SR in older adults due to the combination with heightened levels of internal neural noise.

Similar interaction between external and internal noises has been previously reported both in psychophysics and electrophysiology (Aihara et al., 2010; Douglass et al., 1993). For example, Douglass et al. (1993) found higher-than-expected detection accuracy values in single sensory neurons of crayfish at low external noise levels, proposing that neural noise played a role in this phenomenon. Additionally, Varlet & Richardson (2016) demonstrated a mutual relationship between internal and external noise for neural synchrony, indicating that moderate internal noise facilitates synchronization at minimal external noise levels, whereas high levels of both internal and external noise degrade synchronization.

Considering this theoretical background, our research supports theories suggesting nonlinear effects of neural noise changes on behaviour in noisy environments (Cremer & Zeef, 1987; Li et al., 2001; Welford, 1981), indicating that the effect of increased neural noise, which is marked by enhanced local neural excitability, as evidenced by a decrease in the  $1/f$  exponent, also should be balanced on the levels of external noise.

Research by Tran et al. (2020) demonstrated that older adults with flatter spectral slopes exhibited more variability within the occipital alpha band, as measured by inter-trial phase coherence, indicating an inverse relationship between an increase in neural noise (as a reduction in the exponent of the aperiodic component) and neural variability in response to stimuli. Furthermore, recent findings by Man-yukhina et al. (2024) demonstrated a negative correlation between changes in periodic power and the aperiodic exponent observed before and after a task. This suggests that as the aperiodic exponent decreases (indicating an increase in tonic basal neural noise), there is a corresponding decrease in periodic power.

This interaction implies that heightened neural noise is associated with reduced neural responsiveness at the network level. Additionally, the study highlights a relationship between the aperiodic exponent and poststimulus neural inhibition in visual areas, suggesting that increased neural noise disrupts normal inhibitory processes, leading to altered neural responses following a stimulus. Therefore, an

increase in noise at high frequencies of the spectrum appears to coincide with a disrupted homeostatic balance tipped in favour of excitation, leading to a loss of neural tuning.

According to Rubenstein and Merzenich (2003), cortical noise reflects a hyperexcitable and poorly differentiated cortex. Our findings also align with the Loss of Complexity in Aging Hypothesis (LOCH). Initially, when LOCH was introduced, complexity was defined as the extent to which the underlying system generates aperiodic fluctuations resembling nonlinear chaos. Complexity characterizes a state between order and disorder, where increasing randomness could lead to either an increase or decrease in complexity (Goldberger et al., 2002; Lipsitz & Goldberger, 1992). However, both a reduction in synchronized neural response variability and the increase in aperiodic basal noise could induce a loss of complexity, ultimately leading to decreased behavioural performance (Sleimen-Malkoun et al., 2014). Our study also may represent a support to dedifferentiation theory, according to which age-related decline results from increases in neural noise that reduce the selectivity of neural representations (Reuterr-Lorenz & Park, 2014). Loss of complexity along with dedifferentiation constitute two intertwined facets of the same aging process (Sleimen-Malkoun et al., 2014).

We acknowledge that our conclusions regarding internal noise are preliminary, given that internal noise levels were not directly quantified in our study. Notably, at the beginning of data collection, despite the pandemic abating, it remained inadvisable to involve elderly participants in a laboratory environment. Opting for online testing over in-laboratory assessments allowed for a broader age range, and thus, we employed age as a proxy for increased neural noise. Using age as a proxy for increased neural noise gains support from consistent findings across various independent studies that report a change in exponent with advancing age, underscoring the robustness of this assumption in our research framework. Collectively, these studies suggest a flattening—or reduction—in the exponent with age (Cesnaite et al., 2023; Clark et al., 2024; Dave et al., 2018; Finley et al., 2024; Merkin et al., 2023; Pathania et al., 2022; Tran et al., 2020; Voytek et al., 2015; Waschke et al., 2017), an event linked with an change in the E/I balance (Gao et al., 2017) and an increment in noise at higher frequencies, denoting more local (nonnetwork-level) and asynchronous cortical activity (Thuwal et al., 2021). The recent expansion in such research has been facilitated by the availability of numerous free toolboxes (Donoghue et al., 2020; Hu et al., 2024; Wen & Liu, 2016; Whitten et al., 2011; Wilson et al., 2022), which are integrated into user-friendly analysis platforms. These tools enable straightforward calculations of the exponent and intercept of the aperiodic portion of the EEG spectrum, further applied to investigate the impact of age on basal neural noise. Another limitation is

the nonuniform age distribution in our sample. However, it is reassuring that similar results were observed when analysing age both as a continuous variable, as planned, and as a two-level factor. Lastly, we cannot fully exclude the possibility that differences in hardware typical of online data collection could have impacted data quality, despite the large sample size and rigorous planning of our study.

Future studies could address this limitation, potentially extending and generalizing these results to other tasks, types of noise manipulation, and age cohorts. Furthermore, investigating changes in SR in children and individuals with autism spectrum disorders, characterized by increased neural noise (Dinstein et al., 2012; Milne, 2011; Rubenstein & Merzenich, 2003), would be of interest.

## Conclusions

This study examined age-related changes in psychophysical stochastic resonance in human visual perception, focusing on the impact of external noise. Results confirmed age-related declines in coherent motion detection, aligning with previous findings. Younger participants showed enhanced performance with increased dot numerosity, whereas older adults experienced diminishing advantages, indicating a complex interaction between age, external noise, and task demands.

The investigation into SR revealed an unexpected inverted U-shaped curve, with optimal performance for older individuals occurring at lower external noise levels. This challenges the initial hypothesis and aligns with recent findings by Battaglini et al. (2023). Integrating these results with the neural noise hypothesis of aging suggests that increased internal neural noise may contribute to observed patterns. The interplay between external and internal noise in triggering SR aligns with previous research.

While the reduced ability of older adults to filter external noise may contribute to performance decrements, the speculative nature of conclusions related to internal noise is emphasized because of the absence of direct measurement. Future research should address this limitation, exploring implications in various cognitive tasks and extending findings to diverse populations, such as children and individuals with autism spectrum disorders. This investigation provides valuable insights into nuanced dynamics of age-related changes in visual perception, paving the way for further exploration of the interplay between external and internal noise in the aging brain.

**Authors' contributions** M.D.P., L.B., and G.C. conceived the study. M.D.P. and L.B. contributed to the experimental design. G.C. prepared figures, conducted analysis, and developed the code for data collection. M.D.P., L.B., and M.B. contributed to the interpretation of results.

M.D.P. and G.C. drafted the original manuscript. All authors critically reviewed and approved the final version for submission.

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**Data availability** Data and materials, comprising a demo version of the task, data collection code, and analysis code, are available on the OSF repository. The study was not preregistered.

## Declarations

**Conflicts of interest** The authors have declared that no competing interests exist.

**Ethics approval** The experiment (protocol 4014) received approval from the Ethics Committee of Psychological Research (Area 17) at the University of Padova. The study procedures adhere to the principles outlined in the Declaration of Helsinki.

**Consent to participate** All participants provided informed consent.

**Consent for publication** Participants consented the processing of anonymized and aggregated data for scientific publication.

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